Prediction of Defibrillation Outcome by Ventricular Fibrillation Waveform Analysis: A Clinical Review

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Abstract

The most frequent initial rhythm in out-of-hospital witnessed cardiac arrest is ventricular fibrillation (VF) and electrical defibrillation is still the only effective therapy for the termination of this life-threatening cardiac arrhythmia. Even though earlier defibrillation is greatly emphasized during cardiopulmonary resuscitation (CPR), unnecessary or repetitive high energy defibrillations are associated with decreased post-resuscitation myocardial function. Optimizing the timing of defibrillation is of great importance in order to discriminate patients who should receive immediate defibrillation versus alternate therapies such as CPR. Since characteristics of VF waveform changes over time and with CPR, which exhibit predictable ability of defibrillation success, quantitative analysis of VF waveform has the potential to guide defibrillation. This article reviewed methods developed for VF waveform analysis (including time domain, frequency domain, time-frequency domain, nonlinear analysis, and combination analysis techniques) and their performances for the prediction of defibrillation outcomes in clinical settings. The retrospective meta-analysis confirmed that VF waveform could predict the return of organized electrical activity, restoration of spontaneous circulation, and survival reliably. Additionally, predictors based on time-frequency and nonlinear methods were superior to other methods on the whole. However, no prospective studies have been performed to identify the optimal time of defibrillation utilizing VF waveform analysis until now. Therefore, the value of VF waveform analysis to guide clinical countershock management still needs further investigation.

Keywords: Cardiac arrest; Ventricular fibrillation; Waveform analysis; Defibrillation prediction

Introduction

Ventricular fibrillation (VF), which is characterized as rapid and disorganized contractions of the heart with complex electrocardiogram (ECG) patterns, is the most frequent initial rhythm in out-of-hospital witnessed cardiac arrest (CA) [1]. Electrical defibrillation, which consists of delivering of a therapeutic dose of electrical current to the fibrillating heart with the aid of a defibrillator, is still the only effective way to treat this life-threatening arrhythmia [2]. The probability of defibrillation success is inversely proportional to the duration of VF. Clinical data reported that for every minute passes between collapse and defibrillation, survival rates from witnessed VF decrease 7% to 10% if no cardiopulmonary resuscitation (CPR) is provided. With effective CPR, the success rate of rescue decreases 3-4% per minute [3]. Thus, early CPR together with early defibrillation is a key point in the chain of survival.

The fundamental importance of early defibrillation as a major predictor of outcome in patients with VF has been known since the introduction of external defibrillators [4]. However, emerging evidence showed that not all patients in VF might benefit from being treated in the same manner. Both animal and human studies demonstrated that defibrillation immediately after the onset of VF usually resulted in restoration of spontaneous circulation (ROSC). However, when the duration of untreated VF exceeded 4-5 minutes, initial CPR with chest compression before delivery of a defibrillation attempt improved the likelihood of restoring an organized cardiac electrical activity with pulses [5,6]. Unnecessary shocks can reduce chest compression time and can cause VF to deteriorate into asystole or pulseless electrical activity, which is more difficult to resuscitate [7,8]. On the other hand, repeated futile defibrillation attempts with high energy also associated with myocardial damage and resulting in reduced chance of survival [9]. For these reasons, the ability to gain information concerning the metabolic state of the myocardium and to optimize the timing of defibrillation would be of enormous benefit in allowing therapy to be tailored to an individual heart.

The optimal timing of defibrillation can be determined by evaluating the probability of shock outcome. If the shock attempt has a high likelihood of defibrillation success, an electrical shock should be prompted and delivered. Otherwise, unnecessary shocks should be avoided and alternate therapy such as CPR or medications, especially high-quality chest compression, should be utilized. Earlier investigations established that both the coronary perfusion pressure (CPP) and the end-tidal carbon dioxide (PetCO2) could serve as measurements of the effectiveness of chest compression and therefore as predictors of the likelihood of ROSC [10,11]. But real-time measurements of CPP and PetCO2 are not widely available during out-of-hospital settings.

ECG waveform, which is routinely available in the current automated external defibrillators (AEDs), has been extensively investigated for the purpose of predicting the probability of defibrillation outcome [12]. The ECG signals recorded from the body surface represent the superposition of all of the electrical fields generated by each volume element of the heart [13]. Presumably, the organization of the surface ECG has some relationship to the underlying organization of the myocardial electrical activity. Since characteristics of VF waveform change over time and with CPR, which exhibits ability for prognostication of defibrillation...
success, the quantitative analysis of VF waveform has the potential to be used to predict the VF duration and the probability of shock outcome, to optimize the timing of defibrillation, and to ultimately guide CPR interventions [14].

The observation that defibrillation success rate is higher during the initial period of CA where "coarse VF" with an amplitude greater than 0.2 mV is present, while success of defibrillation is greatly reduced at this stage of "fine VF", is finally evolved to extensive quantitative analysis of ECG waveform [15]. Earlier animal studies demonstrated that duration of CA and defibrillation outcome can be predicted from amplitude and frequency variables obtained from VF waveform [16-19], where the experimental conditions about animals were convenient to be controlled [20]. With widely application of AEDs, various VF analysis techniques, including time domain, frequency domain, time-frequency domain, nonlinear analysis, and combination analysis techniques, have been adapted and developed to predict the probability of defibrillation outcome for patients who experienced out-of-hospital cardiac arrest (OHCA) [21]. In the past 20 years, considerable efforts have been made to further improve the predictive power of rescue shock measures. However, no prospective clinical study has been performed to validate the predictability of VF waveform with real-time analysis. This article reviews the methods used for VF waveform analysis and their performances for the prediction of defibrillation outcomes in clinical settings. The purpose of this study is to compare the advantages of different methods and their reliabilities for optimizing the timing of defibrillation in OHCA patients with retrospective meta-analysis.

Literature Searches

An automatic search was conducted of the following electric databases: PubMed, EMBASE, Web of Science, ScienceDirect, and IEEEXplore, with the keywords such as "defibrillation prediction", "ventricular fibrillation", "waveform analysis", "clinical", and "success countershock". In addition to these automated searchers, a manual search of key articles was conducted as well. All researches published between January, 1985 through March, 2013 were considered. Only papers published in English were included. As a result, a total of 186 literatures were obtained.

For study selection, the publications about myocardial infarction, atrial fibrillation, coronary artery, acute myocardial, waveforms of AEDs, and patients with implantable cardioverter defibrillators (ICDs) were excluded. Moreover, publications focused on the detection of shockable waveform rather than prediction of defibrillation success were also excluded [22,23]. Of the rest literatures, 1 repeated study was removed. As a result, a total of 33 studies that met our selection criteria were finally evaluated. Among the 33 studies, 14, 2, 2, and 2 were published in Resuscitation, Circulation, Annals of Emergency Medicine, and Anesthesia and Analgesia, respectively; the rest 13 studies were published in other medicine journals.

Methods for VF Waveform Analysis

The procedure for the prediction of defibrillation outcome using VF waveform analysis is shown in Figure 1. An episode VF signal with the duration of 1 to 10 seconds, which is immediately before the shock delivery, is usually selected from the surface recording. Due to the fact that preshock pause was independently associated with a decrease in defibrillation efficacy [24], and the recommendation that the delivery of a shock should be achieved with an interruption in chest compressions of no more than 5 seconds by European Resuscitation Council [25] , CPR artifacts may present in the recorded ECG signals. Additionally, the ECG signals recorded from AEDs may also include baseline drifts, powerline interferences, muscle movements, and so on [26-28]. A preprocessing step is usually employed to obtain the 'pure' ECG signals before the waveform analysis, including a notch filter to remove baseline drifting and CPR artifact, and a low-pass filter to remove the myographic noise [29-34]. After filtering, the features or characteristics of the VF signal extracted with different digital signal processing methods are then used to predict the probability of defibrillation success based on the established threshold or decision algorithm.

Based on the digital processing technologies are used, the methods or algorithms used to predict the shock outcome can be categorized into the following five groups: time domain methods, frequency domain methods, time-frequency domain methods, non-linear dynamic methods of randomness and complexity, and the combination of different methods.

Time domain methods

Predictors obtained from time domain describe the characteristics of waveform amplitudes, phases or voltages. Peak-to-peak amplitude (PPA), which is defined as the difference between the maximum and minimum recorded ECG voltage within a given window, was shown to be a powerful indicator of defibrillation outcome by Weaver et al. [15]. Monsieurs and colleagues proposed a survival index, which is calculated as the weighted sum of the VF amplitude and the number of base-line crossings per second, to discriminate potential survivors from non-survivors [35]. The mean amplitude, representing the mean absolute deviation from the mean of the waveform, was used to predict ROSC by Hamprecht and colleagues [36]. Median slope (MdS) and mean slope (MS), which represent the average steepness of the waveform, reflect both the amplitude and frequency information of VF. Joar et al. [37] analyzed the median slope (MdS) in relation to VF duration and the rhythm before onset of VF, which indicated MdS could be used for shock outcome prediction. Neurauter and colleagues studied MdS and MS originated from a range clearly above a lower edge frequency to predict the shock outcome [38]. The extrema of phases, which are defined as the phases of a VF interval immediately before countershock, were found to be sinusoidal with the probability of success defibrillation attempts by Suzuki and colleagues [39].

Amplitude, slope, and phase of VF are not only dependent on the duration of VF but are also affected by other factors: interference, physique, skin resistance, size and position of electrodes, lead ways, and recording conditions [13]. Additionally, the time domain methods do not utilize the temporal information to predict the defibrillation [40]. For these reasons, time-domain features or characteristics are probably crude predictors of defibrillation.

Frequency domain methods

Frequency domain features describe the frequency component characteristics of VF waveform. Each frequency component,
defibrillation outcome prediction by Shandilya and colleagues [28]. Features from dual-tree complex wavelet domain were developed for using logistic regression analysis to predict defibrillation [40].

COP, which yielded the best mixed effects models, for shock outcome technique across hardware platform. Gundersen et al. [47] also adopted Watson and colleagues [49]. Box et al. [55] adopted COP to analyze flatness, and entropy were investigated by Watson and colleagues to temporal information, allowing a local scale-dependent spectral analysis.

Time-frequency domain methods

The continuous or discrete wavelet transform resolves the weakness of frequency domain analysis by providing concomitant spectral and temporal information, allowing a local scale-dependent spectral analysis of signal features. Wavelet-based PF, energy, mean frequency, spectral flatness, and entropy were investigated by Watson and colleagues to predict shock outcome using Bayesian statistics [54].

Cardioversion outcome prediction (COP) (i.e. the wavelet-entropy marker), which is used as a metric of the temporal behavior of the signal, can provide an index for the defibrillation identification by Watson and colleagues [49]. Box et al. [55] adopted COP to analyze the ECG data record and provided confidence in the robustness of the technique across hardware platform. Gundersen et al. [47] also adopted COP, which yielded the best mixed effects models, for shock outcome prediction.

The total mid-band (3–10 Hz) energy spectrum analysis based on continuous wavelet transform was studied by Endoh and colleagues using logistic regression analysis to predict defibrillation [40]. Features from dual-tree complex wavelet domain were developed for defibrillation outcome prediction by Shandilya and colleagues [28].

Non-linear dynamic methods

Earlier researches confirmed that VF is a complex non-linear pattern formed by drifting spiral waves of electrical activity (vortices and rotors) that travel across the myocardium and subsequently break down [56,57]. VF waveform may actually be produced by deterministic mechanisms characteristics of dynamic non-linear system. Early VF was shown to contain an 80-90% deterministic component by a complex mathematical algorithm [58]. There are several reported non-linear features to predict VF defibrillation success, such as the scaling exponent (ScE), Hurst exponent, the logarithm of the absolute correlations (LAC), self-similarity dimension, and detrended fluctuation analysis (DFA).

The ScE is an estimate of the fractal self-similarity dimension. Callaway and colleagues [59] assessed the ability of ScE to predict the success of defibrillation. The Hurst exponent, which is used as a measure of long term memory of time series, was included in a model to predict successful defibrillation attempts by Podbregar et al. [60]. Irregularity, which is a direct indicator of chaotic behavior, was found to be associated with successful defibrillation by Jagric and colleagues [61]. LAC, which quantifies how individual parts of a signal are self-similar at different points along its length, was proposed by Sherman and coauthors to provide prognostic information regarding the duration of VF by measuring the roughness of the VF waveform [62]. DFA, which determines the statistical self-affinity of VF waveform, was used to assess the duration of a VF crisis by Rodriguez et al. [63]. Lin and coauthors [64] applied the DFA on the VF signal analysis to predict the defibrillation success.

Though the VF waveform analysis based on the dynamic non-linear achieved some improvement in predicting successful defibrillation, the non-linear dynamic method is sensitive to the noise and interference.

Combination of several methods

The combinations of individual measurements based on different methods above have also been employed to predict shock outcome. Brown et al. [44] carried out a retrospective analysis of VF signals using 4 features and reported that the combination of FC and PF performed better than other combination and may be used to predict countershock success or to guide therapy during CA. Jekova [65] analyzed a set of 10 parameters reflecting the frequency characteristics, the variations, the complexity, the periodicity and the symmetry of the ECG signals using linear discriminant functions of the 10-dimensional vector. Gundersen and colleagues [47] analyzed 6 predictive features: AMSA, MS, MdS, COP, mean amplitude, and FC using the complete recordings of ECG waveforms. Random effects for each single ECG-feature and the best combination of features performing a forward and a backward search were tested, respectively.

Efstel and colleagues [43,46] combined two decorrelated spectral features based on the principal component analysis (PCA) of an original feature set with information on FC, peak power frequency, spectral flatness and energy, using multidimensional information in a single reproducible variable reflecting the probability of defibrillation success. Watson and colleagues [54] analyzed the performance gained through the combination of PF, energy, mean frequency, spectral flatness, and entropy measure, when PCA was applied to the combination of features. Podbregar and colleagues [60] studied the predictive power of a model developed by genetic programming (GP) on the complete VF database including maximal amplitude, total energy of power spectral density, and the Hurst exponent to predict defibrillation success.
Neurauter and colleagues [38] applied neural networks on single-feature combinations to optimize the prediction of countershock success. Time domain features (e.g. mean amplitude, PPA, and MS) and frequency domain features (e.g. PF, centroid power, and the PSA) were calculated from the re-countershock VF ECG signal. Shandilya and colleagues [28] focused on time-series and complex wavelet integration of multiple features through machine learning techniques, training and testing 6-10 features for each test fold with nested 10-fold cross validation. Identification of the most discriminative features and correlated variables were conducted by the supervised feature selection. A parametrically optimized support vector machine model was trained for predicting outcomes.

The combination method synthesizes several single features by linear discriminant functions, neural networks, GP, and so on. Thus, the computing power is prodigious and time consuming, which may not satisfy the computational requirement of AEDs.

Results

Definition of defibrillation success

There is no consistent definition of defibrillation success of the related publications [28]. According to the literatures, two definitions were commonly adopted in the studies of countershock prediction as standard of successful defibrillation: (1) defibrillation was considered to be successful with resulting in an organized rhythm seen at 5 second after delivery of the shock regardless of palpated pulsation of the common carotid artery by Koster et al. [66]; (2) successful defibrillation was defined as those attempts which result in ROSC sustained for a period greater than 30 seconds and originating within a minute of the applied shock by Watson et al. [49].

In this clinical review, we broadly classify outcomes into three categories based on the definitions of defibrillation success in each article. The first one is return of organized electrical activity (ROEA) at least 5 seconds following countershock including termination of the VF and return of a stable supraventricular rhythm, termed as Definition 1. The second one is ROSC, which generates a pulse regardless of the duration at least 30 s without continuing CPR, termed as Definition 2. The palpated pulsation of the common carotid artery is an important sign of ROSC differing from the ROEA. The third one is the most rigorous definition, as the survival at least 6 hours after resuscitation or with discharge from the hospital, termed as Definition 3.

According to the three categories of definition of successful defibrillation, the clinical performances of defibrillation predictors are listed in the following three tables. Table 1 corresponds to Definition 1, Table 2 presents the results according to Definition 2, and Table 3 shows the performances using Definition 3. Only the predictor with the best performance is listed in the three tables, if several predictors were analyzed in one study.

Retrospective analysis results

Results of different defibrillation prediction methods in the literatures are commonly presented in terms of sensitivity, specificity, and area under receiver operating curve (ROC) curve (AUC). Sensitivity is defined as the proportion of shocks that are successfully defibrillated which are correctly identified, specificity is the proportion of failed shocks that are correctly identified [49], and AUC is defined as the area under the ROC curve. A trade-off in sensitivity and specificity achievable by a system is described by plotting sensitivity/specificity pairs in a ROC curve. AUC provides an indication of the system effectiveness. The larger the AUC value is, the better the system performance presents. An ideal case is that an area equals to unity where sensitivity is one for all specificities. Other unusually criteria such as the accuracy [28], the odds ratio (OR) [67], and the Wald value [40] that adopted to evaluate the performances of different defibrillation predictors were not analyzed in our results.

A total of 7 studies reported their data according to Definition 1 (Table 1). Sensitivity ranges from 61% to 100% with an averaged value of 87.4%, specificity ranges from 14% to 97% with the averaged value 55.3%. Among the 7 features, MR, PPA, PF and a combination by GP achieve the highest sensitivity 100%. A combination by GP achieves the highest specificity 97%. Two studies reported their results of AUC, with 0.65 for DFA and 0.77 for FC based on CWT.

A total of 20 studies reported their data according to Definition 2 (Table 2). Sensitivities range from 59% to 100% with the averaged value 89.7%, COP and a combination of PF and FC achieve the highest sensitivity 100%. Specificities range from 32% to 97% with the averaged value 61.2%. Among the 14 investigated features, AMSA achieves the highest specificity of 97%. AUC values range from 0.77 to 0.94 with the averaged value 0.86. The feature based on complex wavelet transform with addition of the PetCO2 signal achieves the highest AUC of 0.94.

A total of 6 studies reported their data according to Definition 3 (Table 3). Sensitivities range from 54% to 96.7% with the averaged value 78.4%, PPA achieves the highest sensitivity 96.7%. Specificities range from 22.7% to 98% with the averaged value 70.7%. Among the 5 investigated features, PPA achieves the highest specificity 98%. The only reported AUC value is 0.84 achieved by SE.

Meta-analysis (Review Manager 5.2.4) was utilized to evaluate the effects of successful defibrillation definition and methods used for VF waveform analysis on the performance of the predictability. All of the predictors were included for meta-analysis to enhance the reliability if more than 1 indicator was investigated for each study.

The results of meta-analysis based on the definition of defibrillation success are listed in Table 4. Characteristics of VF waveform can reliably predict defibrillation outcome with the use of definition of ROEA, ROSC and survival. The odds ratio (OR) for prediction of ROEA is significantly higher than those of ROSC and survival. The results listed in Table 5 revealed that time-frequency and nonlinear methods outperformed other techniques with relative higher OR when ROSC is served as shock outcome.

Discussion

The duration of VF is a major determinant of counter shock outcome. However, it is difficult to establish the prior duration of VF in clinical settings. An ideal predictor of defibrillation shock outcome would enable the rescuers to provide the most appropriate therapy for the patient, and could be implemented into existing AEDs with less computing power. Many clinical studies have been performed to measure the characteristics of VF waveform and predict the likelihood of successful defibrillation. However, there is still no clinical standard has been postulated as the threshold of the reliability of shock prediction.

A sensitivity of 95% and specificity of 50% was suggested as safe and useful predictor for the treatment of VF by Neurauter et al. [38,73]. Based on the reported results, a combination of PPA, total energy of PSD and Hurst exponent with GP algorithm outperformed other indicators for the prediction of ROEA, with a sensitivity of 100% and specificity...

<table>
<thead>
<tr>
<th>Year</th>
<th>Author</th>
<th>Predictor</th>
<th>Data</th>
<th>AUC</th>
<th>SES(%)</th>
<th>SPE(%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1991</td>
<td>Dalzell et al. [68]</td>
<td>PPA</td>
<td>70 patients within or outside hospital</td>
<td>/</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>1994</td>
<td>Strohmenger et al. [48]</td>
<td>MF</td>
<td>20 patients during aortocoronary bypass grafting</td>
<td>/</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>1997</td>
<td>Strohmenger et al. [45]</td>
<td>PPA and PF</td>
<td>26 patients with OHCA</td>
<td>/</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>2003</td>
<td>Podbregar et al. [60]</td>
<td>Combination of PPA, total energy of PSD and Hurst exponent by GP</td>
<td>47 patients with OHCA (79 success shock, and 124 unsuccessful shock)</td>
<td>/</td>
<td>100</td>
<td>97</td>
</tr>
<tr>
<td>2010</td>
<td>Lin et al. [64]</td>
<td>DFA(DFAα2)</td>
<td>155 OHCA subjects (37 successful and 118 unsuccessful defibrillations)</td>
<td>0.65</td>
<td>61</td>
<td>63.2</td>
</tr>
<tr>
<td>2011</td>
<td>Endoh et al. [40]</td>
<td>FC based on CWT</td>
<td>152 patients with OHCA (164 unsuccessful and 69 successful episodes)</td>
<td>0.77</td>
<td>76.8</td>
<td>62.8</td>
</tr>
<tr>
<td>2012</td>
<td>Shanmugasundaram et al. [67]</td>
<td>Slope</td>
<td>44 patients with OHCA: In recurrent VF /</td>
<td>91</td>
<td>/</td>
<td>14</td>
</tr>
</tbody>
</table>

SES, sensitivity; SPE, specificity; "/ " denotes the corresponding values were not reported.

Table 1: Performance of defibrillation predictors using Definition 1.

<table>
<thead>
<tr>
<th>Year</th>
<th>Author</th>
<th>Predictor</th>
<th>Data</th>
<th>AUC</th>
<th>SES(%)</th>
<th>SPE(%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1991</td>
<td>Martin et al. [50]</td>
<td>MF</td>
<td>7 patients / / /</td>
<td>/</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>1996</td>
<td>Brown et al. [44]</td>
<td>Combination of PF and FC in certain ranges</td>
<td>55 patients with OHCA /</td>
<td>100</td>
<td>47.1</td>
<td>/</td>
</tr>
<tr>
<td>2000</td>
<td>Eftestol et al. [46]</td>
<td>Combination of FC and PF</td>
<td>156 patients with OHCA (total 868 shocks;87 had caused ROSC and 781 had failed to cause ROSC )</td>
<td>/</td>
<td>92 ± 2</td>
<td>42 ± 1</td>
</tr>
<tr>
<td>2001</td>
<td>Strohmenger et al. [69]</td>
<td>DF</td>
<td>89 patients with OHCA /</td>
<td>92</td>
<td>/</td>
<td>42</td>
</tr>
<tr>
<td>2001</td>
<td>Eftestøl et al. [43]</td>
<td>Combination of CF and the energy</td>
<td>156 patients with OHCA (total 883 shocks;87 had caused ROSC and 781 had failed to cause ROSC )</td>
<td>/</td>
<td>91 ± 3</td>
<td>36 ± 4</td>
</tr>
<tr>
<td>2001</td>
<td>Hamprecht et al. [36]</td>
<td>DF</td>
<td>54 patients with OHCA (artefact-free ventricular fibrillation episodes, 26 return to ROSC)</td>
<td>/</td>
<td>59</td>
<td>52</td>
</tr>
<tr>
<td>2004</td>
<td>Jekova et al. [70]</td>
<td>Energy between 2 and 7 Hz</td>
<td>more than 700 out-of-hospital fibrillation cases /</td>
<td>61.8</td>
<td>79.6</td>
<td>/</td>
</tr>
<tr>
<td>2004</td>
<td>Young et al. [51]</td>
<td>AMSA</td>
<td>46 patients with OHCA /</td>
<td>91</td>
<td>/</td>
<td>94</td>
</tr>
<tr>
<td>2004</td>
<td>Watson et al. [54]</td>
<td>Entropy measure based on Morlet wavelet</td>
<td>87 success shock and 781 unsuccess shock /</td>
<td>91 ± 2</td>
<td>60 ± 6</td>
<td></td>
</tr>
<tr>
<td>2005</td>
<td>Watson et al. [49]</td>
<td>COP based on a tunable Morlet wavelet</td>
<td>110 patients with OHCA /</td>
<td>97 ± 2</td>
<td>63 ± 4</td>
<td></td>
</tr>
<tr>
<td>2006</td>
<td>Watson et al. [71]</td>
<td>COP based on CWT</td>
<td>110 patients with OHCA /</td>
<td>95 ± 4</td>
<td>66 ± 4</td>
<td></td>
</tr>
<tr>
<td>2007</td>
<td>Neurauter et al. [38]</td>
<td>MdS</td>
<td>197 patients with in-hospital and out-of-hospital CA</td>
<td>0.848</td>
<td>95.2</td>
<td>52.6</td>
</tr>
<tr>
<td>2007</td>
<td>Jagic et al. [81]</td>
<td>Irregularity</td>
<td>120 recordings of VF /</td>
<td>/</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>2007</td>
<td>Cunderson et al. [47]</td>
<td>COP</td>
<td>86 patients with OHCA /</td>
<td>0.877</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>2008</td>
<td>Box et al. [55]</td>
<td>COP based on wavelet transform</td>
<td>54 patients with OHCA /</td>
<td>100</td>
<td>60</td>
<td>/</td>
</tr>
<tr>
<td>2008</td>
<td>Sherman et al. [62]</td>
<td>LAC</td>
<td>158 patients with OHCA /</td>
<td>0.77</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>2008</td>
<td>Ristagno et al. [72]</td>
<td>AMSA</td>
<td>90 patients with OHCA /</td>
<td>91</td>
<td>97</td>
<td></td>
</tr>
<tr>
<td>2008</td>
<td>Neurauter et al. [73]</td>
<td>MdS(10-22Hz)</td>
<td>192 patients with in-hospital and out-of-hospital CA</td>
<td>0.863</td>
<td>95.2</td>
<td>49.7</td>
</tr>
<tr>
<td>2012</td>
<td>Nakagawa et al. [74]</td>
<td>AMSA</td>
<td>93 patients with OHCA /</td>
<td>94</td>
<td>59</td>
<td>/</td>
</tr>
<tr>
<td>2012</td>
<td>Shandilya et al. [28]</td>
<td>Feature based on complex wavelet transform</td>
<td>57 patients (34 successful and 56 unsuccessful defibrillations) ECG signals without addition of the PetCO2 signal With addition of the PetCO2 signal</td>
<td>0.850</td>
<td>90</td>
<td>78.6</td>
</tr>
</tbody>
</table>

SES, sensitivity; SPE, specificity; "/ " denotes the corresponding values were not reported.

Table 2: Performance of defibrillation predictors using Definition 2.

<table>
<thead>
<tr>
<th>Year</th>
<th>Author</th>
<th>Predictor</th>
<th>Data</th>
<th>AUC</th>
<th>SES(%)</th>
<th>SPE(%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1985</td>
<td>Weaver et al. [15]</td>
<td>PPA</td>
<td>394 patients / / /</td>
<td>/</td>
<td>96.7</td>
<td>22.7</td>
</tr>
<tr>
<td>1992</td>
<td>Stewart et al. [41]</td>
<td>PF</td>
<td>56 patients in hospital and in the community /</td>
<td>/</td>
<td>/</td>
<td>/</td>
</tr>
<tr>
<td>1998</td>
<td>Monsieurs et al. [35]</td>
<td>Survival index</td>
<td>100 patients with OHCA If adding age /</td>
<td>79</td>
<td>70</td>
<td>/</td>
</tr>
<tr>
<td>2003</td>
<td>Goto et al. [42]</td>
<td>DF</td>
<td>47 patients with OHCA /</td>
<td>76.5</td>
<td>90</td>
<td>/</td>
</tr>
<tr>
<td>1993</td>
<td>Callaham et al. [75]</td>
<td>PPA</td>
<td>265 patients in prehospital VF /</td>
<td>54</td>
<td>/</td>
<td>98</td>
</tr>
<tr>
<td>2001</td>
<td>Callaway et al. [59]</td>
<td>SE</td>
<td>75 subjects with OHCA /</td>
<td>0.84</td>
<td>/</td>
<td>/</td>
</tr>
</tbody>
</table>

SES, sensitivity; SPE, specificity; "/ " denotes the corresponding values were not reported.

Table 3: Performance of defibrillation predictors using Definition 3.
post-resuscitation cerebral injury and myocardial dysfunction. Post-resuscitation care interventions such as therapeutic hypothermia can significantly improve both the neurological recovery and survival after resuscitation from CA.

**Limitation**

There are several limitations need to be addressed for this review analysis. Firstly, the durations of VF waveform that used to be analyzed are different from individual studies. According to the reported results, an episode of 1 to 10 seconds is usually selected from the surface ECG. However, effect of window length on the performance has not been systematically investigated. Secondly, although the filtered ECG signals or CPR-artifact-free ECG signals are reported to have better results than the ECG signals with CPR artifacts and without preprocessing, whether the application of different filtering methods, such as adaptive filtering improve the predictability is still unknown. Thirdly, the waveform design is significantly differ among manufactures, therefore the reliability of VF waveform analysis with the use of different defibrillation waveforms needs to be researched. Fourthly, meta-analysis revealed that time-frequency and nonlinear methods are superior to other techniques, but only a few papers present results of direct comparisons between various methods. The interpretation may be biased due to different patient number, analytical measurement and post-shock annotations.

**Conclusion**

Recent clinical studies verified that it is possible to predict defibrillation success from the VF waveform with varying reliability. Digital signal processing techniques based on amplitude, slope, spectrum, energy, wavelet transform, fractal, entropy, advanced machine learning, and so on, have been applied/proposed to extract features and make decisions for the optimal timing of defibrillation based on surface ECG waveform. Among these techniques, time-frequency and nonlinear methods outperform time domain and frequency domain methods. A better performance is obtained for the prediction of defibrillation success with a short term outcome definition, i.e. ROEA. The combination of single features derived from VF waveform does not further increase the predictability. But the performance of defibrillation predictors may be improved by incorporating patient information and other physiological measurements.

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**Conflict of interest statement**

The authors have no conflicts of interest to disclose.

**References**


